

HEALTHCARE MATERIALS

Syndesome Therapeutics for Enhancing Diabetic Wound Healing

Subhamoy Das, Gunjan Singh, Marjan Majid, Michael B. Sherman, Somshuvra Mukhopadhyay, Catherine S. Wright, Patricia E. Martin, Andrew K. Dunn, and Aaron B. Baker*

Chronic wounds represent a major healthcare and economic problem worldwide. Advanced wound dressings that incorporate bioactive compounds have great potential for improving outcomes in patients with chronic wounds but significant challenges in designing treatments that are effective in long-standing, nonhealing wounds. Here, an optimized wound healing gel was developed that delivers syndecan-4 proteoliposomes ("syndesomes") with fibroblast growth factor-2 (FGF-2) to enhance diabetic wound healing. In vitro studies demonstrate that syndesomes markedly increase migration of keratinocytes and fibroblasts isolated from both nondiabetic and diabetic donors. In addition, syndesome treatment leads to increased endocytic processing of FGF-2 that includes enhanced recycling of FGF-2 to the cell surface after uptake. The optimized syndesome formulation was incorporated into an alginate wound dressing and tested in a splinted wound model in diabetic, ob/ob mice. It was found that wounds treated with syndesomes and FGF-2 have markedly enhanced wound closure in comparison to wounds treated with only FGF-2. Moreover, syndesomes have an immunomodulatory effect on wound macrophages, leading to a shift toward the M2 macrophage phenotype and alterations in the wound cytokine profile. Together, these studies show that delivery of exogenous syndecan-4 is an effective method for enhancing wound healing in the long-term diabetic diseased state.

angiopathy are common complications of diabetes and contribute to a 12%-25% lifetime risk of developing diabetic ulcers.^[1] These diabetic ulcers are responsible for 25%-50% of the total cost of diabetes treatment and are the most common cause of limb amputations in the United States.^[2] Nonhealing, diabetic ulcers are a complex clinical problem requiring a multifaceted treatment plan with standard therapeutic components including removal of necrotic tissue from wound (debridement), reduction of pressure in the wound (offloading), infection control, surgical revascularization, and limb elevation or compression. However, in many cases these treatments are ineffective, leaving patients with chronic ulcers and enhanced risk for limb amputation.

A number of advanced wound dressings have been used to enhance healing of chronic ulcers. The most prevalent approaches to bioactive dressings can be broadly classified into the categories of local delivery of growth factors,^[3] delivery of therapeutic genes,^[4] or delivery of stem cells.^[5] Of these strategies, only growth

1. Introduction

Type 2 diabetes is a highly prevalent disorder that impacts 347 million people worldwide. Neuropathy and microvascular

Dr. S. Das, G. Singh, M. Majid, Prof. A. K. Dunn, Prof. A. B. Baker Department of Biomedical Engineering University of Texas at Austin Austin, TX 78731, USA E-mail: abbaker@austin.utexas.edu Prof. M. B. Sherman Department of Biochemistry and Molecular Biology University of Texas Medical Branch Galveston, TX 77555, USA S. Mukhopadhyay Division of Pharmacology and Toxicology

University of Texas at Austin Austin, TX 78731, USA S. Mukhopadhyay

Institute for Neuroscience University of Texas at Austin Austin, TX 78731, USA

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factors have been tested in large clinical trials, perhaps due to the safety and logistical challenges accompanying gene or stem cell therapies. However, the vast majority growth factor therapies have limited success in clinical trials for wound

Prof. S. Mukhopadhyay, Prof. A. B. Baker Institute for Cellular and Molecular Biology University of Texas at Austin Austin, TX 78731, USA Dr. C. S. Wright, Prof. P. E. Martin Diabetes Research Group Department of Life Sciences and Institute for Applied Health Research Glasgow Caledonian University Glasgow G4 0BA, UK Dr. A. B. Baker The Institute for Computational Engineering and Sciences University of Texas at Austin Austin, TX 78731, USA Prof. A. B. Baker Institute for Biomaterials, Drug Delivery and Regenerative Medicine University of Texas at Austin Austin 78731, USA



healing.^[6] The only approved clinical growth factor treatment for chronic wounds is recombinant platelet derived growth factor-BB (PDGF-BB; Becaplermin), and, while approved by the Food and Drug Administration (FDA), it has shown mixed results in clinical trials on chronic ulcers.^[7] Other growth factors including fibroblast growth factor-2 (FGF-2) and epidermal growth factor (EGF) have either shown no improvement or only moderate benefits in small clinical trials.^[8] Thus, while clinical studies have shown that growth factor therapies are well tolerated by patients, there is a pronounced need to improve the efficacy of these treatments to maximize the benefit of these therapies and make them cost effective for our healthcare system.

Here, we hypothesized that the diabetic state prevents the effectiveness of growth factor therapies through alterations in expression and proteolytic degradation of receptors and coreceptors. This concept is supported by reduced efficacy of growth factors in many clinical trials for enhancing healing in chronic wounds^[8] compared to healthy animals.^[9] In addition, our group recently examined the expression of growth factor receptors and co-receptors in the heart and skeletal muscle of diabetic mice and found a significant loss in syndecan-4 and other cell surface proteoglycans that serve as co-receptors for growth factors including FGF-2, vascular endothelial growth factor-A (VEGF-A), and platelet derived growth factor-CC (PDGF-CC).^[10] We have also shown that diabetes and other disease states increase expression of heparanase, an enzyme that cuts the heparan sulfate chains and increases shedding of cell surface proteoglycans.^[11,12] In this study, we demonstrate that there is a reduction in syndecan-4 in the skin of human patients with type 2 diabetes. We examined whether delivery of syndecan-4 proteoliposomes ("syndesomes") could overcome the inherent resistance to growth factor signaling to enhance the healing of wounds in diabetic mice with severe disease. Our studies show that syndesomes delivered locally from alginate wound dressings markedly enhanced the efficacy of FGF-2 therapy for wound healing in the diabetic disease state through multiple mechanisms.

2. Results

2.1. Syndecan-4 is Reduced in the Skin of Patients with Type 2 Diabetes

We hypothesized that the long-term disease state of diabetic patients may reduce the levels of syndecan-4 and thus reduce the effectiveness of growth factor therapies in this patient population. To examine whether there was loss of syndecan-4 in diabetic humans, we collected skin samples from patients with type 2 diabetes and nondiabetic patients (Table S1, Supporting Information), and then performed immunostaining of syndecan-4 in these tissues. We found a significant reduction in the staining of syndecan-4 in both the overall tissue samples (**Figure 1**A) and in the blood vessels (Figure 1B). We next aimed to examine whether syndesomes would be able to overcome enhance FGF-2 activity in the context of the diabetic disease state in which there is a loss of syndecan-4 and reduced



responsiveness to growth factor therapy. The overall concept was to deliver FGF-2 with liposomes incorporating syndecan-4 (syndesomes) from a nonadhesive alginate wound dressing that could be applied to nonhealing wounds in diabetic patients for enhancing wound healing (**Figure 2**).

2.2. Synthesis and Characterization of Syndesomes and Alginate Gels

We created syndesomes by isolating recombinant syndecan-4 proteins and fusing them into the membrane of liposomes using a detergent extraction method. We confirmed the purity of the syndecan-4 protein using sodium dodecyl sulfate-polyacrylamide electrophoresis (SDS-PAGE) with silver staining as well as western blotting for syndecan-4 (Figure S1, Supporting Information). A high molecular weight smear was observed in the blots implying that majority of the syndecan-4 was glycosylated. We also measured the size distribution of the isolated recombinant protein and the syndesomes using dynamic light scattering. This analysis demonstrated that the recombinant protein in isolation had significant self-association and separated into three distinct peaks, most likely representing protein aggregate formation and varying degrees of glycosylation (Figure 1D). In contrast, the syndesomes had a single distinct peak corresponding to the approximate liposome diameter of 400 nm. In addition, we confirmed the integrity of the liposomes by performing cryo-electron microscopy (cryo-EM) analysis of the liposomes and syndesomes (Figure 1E). To further confirm the incorporation of the protein into the lipid membrane, we examined the change in size of the liposome with varying amounts of protein using transmission electron microscopy. We measured the amount of syndecan-4 before and after incorporation into liposomes and found the majority of the protein was associated with the liposomes after detergent removal (98% ± 2% protein encapsulation; n = 3). We found that the liposome size increased with increasing amounts of protein incorporation (Figure S2A, B, Supporting Information). In addition, the zeta potential of the liposomes was altered by syndecan-4 incorporation (Figure S2C, Supporting Information). To create a local delivery platform for release of the syndesomes into the wound, we encapsulated the compounds into alginate disks (Figure 1F). The release kinetics of FGF-2 from the alginate was similar over the implantation time of 7 d (Figure 1G). We confirmed that the proteoliposomes were released intact by measuring the size of the released liposomes before and after release with dynamic light scattering (DLS; Figure S3, Supporting Information).

2.3. Syndesomes Enhance Keratinocyte Migration and Reduce Both Fibroblast Invasion and Migration

We next assessed whether exogenous delivery of syndecan-4 could enhance the migration and invasion of dermal fibroblasts and keratinocytes, two key cellular effectors of wound healing. Keratinocytes from nondiabetic donors showed a

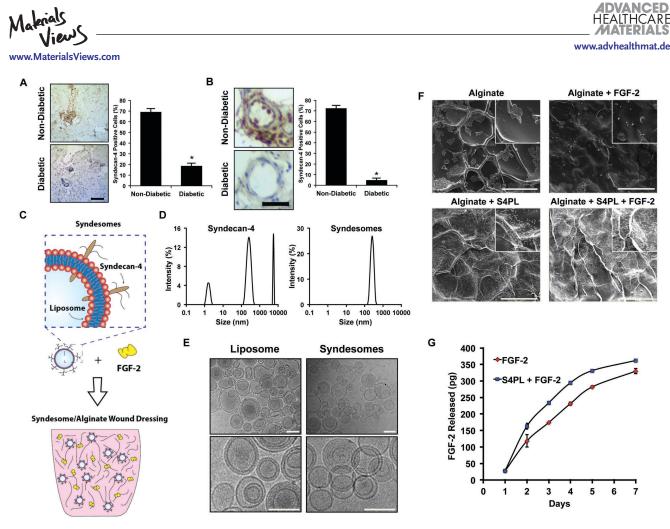


Figure 1. Measurement of syndecan-4 levels in the skin of diabetic and healthy patients; synthesis and characterization of syndesomes. A) Expression of syndecan-4 in human skin from diabetic and nondiabetic patients for the overall skin histology. Bar = 25 μ m. B) Expression of syndecan-4 in the blood vessels in the human skin. Bar = 25 μ m. C) Diagram of incorporating syndesomes and FGF-2 in an alginate wound dressing. D) Dynamic light scattering analysis for syndecan-4 protein and liposomes incorporated with syndecan-4 (syndesomes). E) Cryo-electron microscopy images liposomes and syndesomes. Bar = 400 nm. F) Scanning electron microscopy images of desiccated alginate disks with various treatments. Bar = 100 μ m. G) Release kinetics of the FGF-2 from alginate beads containing syndesomes with FGF-2 or FGF-2 alone. *Statistically different from the nondiabetic patient group (p < 0.05, n = 9).

nearly fourfold increase in migration with treatment with the syndecan-4 proteoliposomes at the optimal concentration (0.2% S4PL; Figure 2A). Surprisingly, the syndesomes alone were more effective at inducing migration than in combination with FGF-2 but migration was increased under both conditions. Keratinocytes from diabetic patients showed only a moderate increase in migration in the groups treated with both syndecan-4 and FGF-2 (Figure 2B). Higher doses of syndecan-4 with FGF-2 demonstrated a reduction in migration for both cell lines. In contrast, treatment with the syndesomes appeared to decrease migration of normal dermal fibroblasts (Figure 2C) and did not alter the migration of fibroblasts from diabetic patients (Figure 2D). We also measured the invasion of fibroblasts through a collagen gel under various treatment conditions and found a moderate reduction in migration with syndesome treatment in diabetic fibroblasts and no significant difference between the treatment groups in the normal fibroblasts (Figure S4, Supporting Information).

2.4. Syndesomes Increase Endosomal Processing and Recycling of FGF-2 to the Cell Surface

FGF-2 can be internalized by receptor-mediated and heparan sulfate proteoglycan-mediated mechanisms. The FGF receptor-1 (FGFR1) is endocytosed into early endosomes in a both a caveolin and clathrin-dependent mechanisms, from which it can be recycled through both the slow and fast pathways, or shuttled to the lysosomal compartment for degradation.^[13] We next investigated how syndesomes altered the endosomal processing of FGF-2 to better understand the mechanism of action. Cells were transfected with plasmids containing green fluorescent protein (GFP) conjugated Rab proteins to label specific endosome subsets and then treated with fluorescently labeled FGF-2. We quantified the percentage of endosomes that co-localized with labeled FGF-2 for each time point. We found a significant increase in percentage of Rab5 (early endosome marker) labeled endosomes with FGF-2 in the syndesome with FGF-2 group at all the time points indicating



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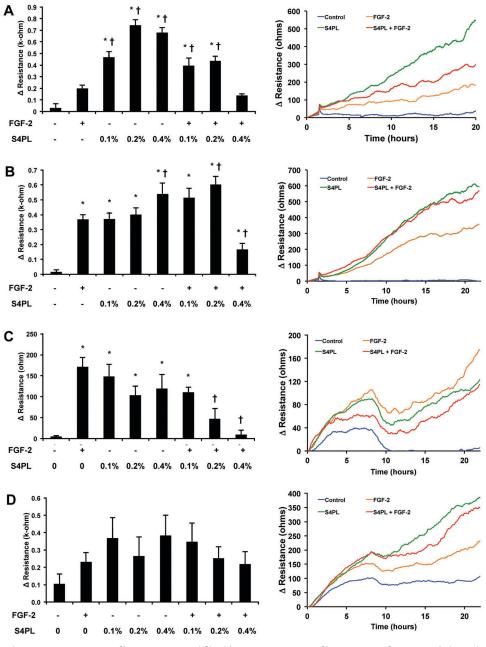


Figure 2. Effect of syndesomes on migration of keratinocytes and fibroblasts. A) Migration of keratinocytes from a nondiabetic donor at the 20 h, with various treatments shown as bar graphs (left). Line graphs showing the time course of the change of resistance for the four treatment groups (right). Note that S4PL concentration is 0.4%. B) Migration of keratinocytes from a diabetic donor at the 20 h, with various treatments shown as bar graphs (left). Line graphs showing the time course of the change of resistance for the four treatment groups (right). Note that S4PL concentration is 0.4%. C) Change in resistance due to migration at 20 h in dermal fibroblasts from a nondiabetic donor, shown as bar graphs (left). Line graphs show the time course of the change of resistance for all the treatments with 0.4% S4PL concentration (right). D) Change in resistance due to migration at 20 h in dermal fibroblasts from a diabetic donor, shown as bar graphs (left). Line graphs show the time course of the change of resistance for all the treatments with 0.4% S4PL concentration (right). *p < 0.05 compared with no treatment group and $^{\dagger}p < 0.05$ compared with the FGF-2 group.

higher FGF-2 uptake (Figure 3A). The level of FGF-2 that colocalized with the late endosomal marker Rab7 (late endosomal marker) remained low throughout the experiment, showing significant differences between the treatment groups only at 120 min (Figure 3B). There was an increase in the percentage of FGF-2 positive Rab11 endosomes (late recycling endosomes) at all time points when we compare the FGF-2 only treatment with the syndesomes with FGF-2 treatment (Figure 3C). Thus, the majority of the FGF-2 that was processed through endosomal pathways was likely getting recycled to the plasma membrane surface through the Rab11 pathway rather than getting degraded by the Rab7 pathway. This hypothesis was supported by a significant increase in the Rab4 endosomes (early recycling endosomes) co-localizing with FGF-2 in the syndesome with



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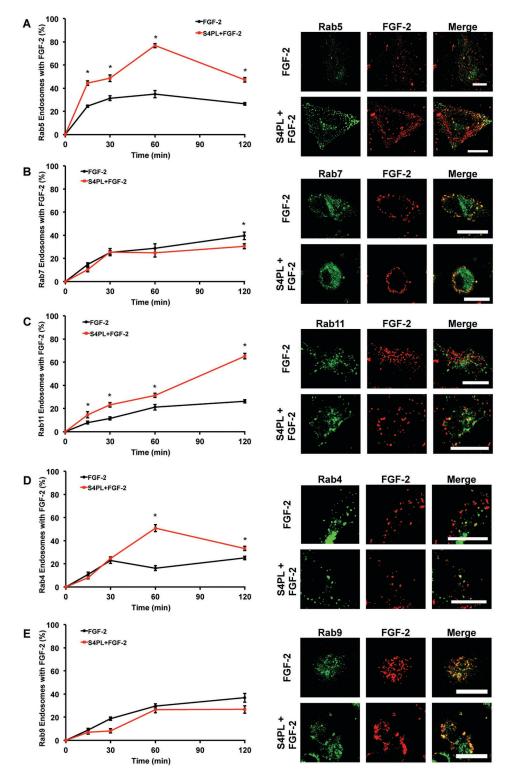


Figure 3. Syndesomes alter endosomal processing of FGF-2. HEK cells were transfected with GFP-Rab5, GFP-Rab7, and GFP-Rab11 separately. These cells were treated with AF594-labeled FGF-2 and syndesomes. A) Percentage of Rab5 endosomes that co-localize with labeled FGF-2 with or without syndesomes. The image panel shows GFP-Rab5, AF594 FGF-2 and merged channels for the two treatments. B) Percentage of Rab1 endosomes that co-localize with labeled FGF-2 with or without syndesomes. The image panel shows GFP-Rab11 endosomes that co-localize with labeled FGF-2 with or without syndesomes. The image of Rab11 endosomes that co-localize with labeled FGF-2 with or without syndesomes. The image panel shows GFP-Rab11 endosomes that co-localize with labeled FGF-2 with or without syndesomes. D) Percentage of Rab4 endosomes that co-localize with labeled FGF-2 with or without syndesomes. The image panel shows GFP-Rab4, AF594 FGF-2 and merged channels for the two treatments. E) Percentage of Rab9 endosomes that co-localize with labeled FGF-2 with or without syndesomes. The image panel shows GFP-Rab4, AF594 FGF-2 and merged channels for the two treatments. E) Percentage of Rab9 endosomes that co-localize with labeled FGF-2 with or without syndesomes. The image panel shows GFP-Rab9, AF594 FGF-2 and merged channels for the two treatments. E) Percentage of Rab9 endosomes that co-localize with labeled FGF-2 with or without syndesomes. The image panel shows GFP-Rab9, AF594 FGF-2 and merged channels for the two treatments. E) Percentage of Rab9 endosomes that co-localize with labeled FGF-2 group at the same time point (p < 0.05; n = 10).



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FGF-2 group (Figure 3D). We did not see any differences in the co-localization of Rab9 endosomes (late endosomes that transport to trans-golgi network) with FGF-2 (Figure 3E).

2.5. Syndesomes Improve Wound Healing in Obese, Diabetic Mice

We next tested the effectiveness of syndesome therapy for enhancing wound healing in the diabetic ob/ob mouse model. Previous studies have shown that these mice have reduced wound closure^[14] and have reduced responsiveness to FGF-2,^[15] when placed on a high fat diet. To examine whether syndesomes could enhance wound healing in a diabetic and obese animal model, we created full-thickness wounds on the dorsal surface of these mice and attached a silicone splint around the wound using glue and sutures to prevent contraction. We created alginate wound dressings that matched the size of the wounds using a custom-designed mold (Figure 4A). The gels were replaced seven days after the initial wounding and the mice were allowed to heal for an additional seven days. A macroscopic analysis of wound closure revealed a twofold decrease in wound size after 14 d in the syndesomes with FGF-2 treatment compared to FGF-2 alone (Figure 4B,C and Figure S5A,B, Supporting Information). We performed immunostaining for cytokeratin and measured the regeneration of the epidermis beyond the initial wound defect. A morphometric quantification showed increase re-epithelization in the syndesome with FGF-2 group over the other treatment groups (Figure 4D,E). Analysis of the granulation tissue area revealed similar levels of granulation tissue in all wounds with a slight increase in the FGF-2 treated samples (Figure S5C,D, Supporting Information). A histological analysis of the wound beds demonstrated increased cellular infiltration in the syndesome with FGF-2 group in comparison to the other groups including the syndesomes alone (Figure 4F).

2.6. Syndesomes Increase Perfusion in the Healing Wound Bed

We measured the blood perfusion in the wounds immediately after wounding and seven days later. Due to the variation in healing between the groups we did not measure blood perfusion in the wounds at day 14 following wounding. We found that there was significant increase of blood perfusion in the syndesomes with FGF-2 compared to all other groups at seven days (**Figure 5A**,B). After 14 d, we harvested the wound beds and performed immunostaining for endothelial cells. This analysis showed increased blood vessels in the wound bed of the FGF-2 with syndesome treated group in comparison to FGF-2 alone and other groups (Figure 5C,D).

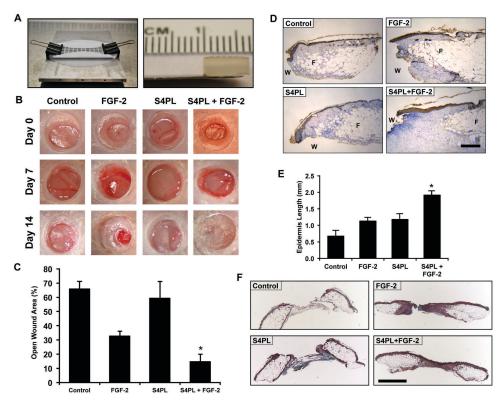


Figure 4. Syndesomes enhance cutaneous wound healing in ob/ob mice on high fat diet. A) Custom-made mold for fabricating alginate disks and the alginate disk. B) Macroscopic images of wound closure over 14 d with various treatments. C) Quantification of the open wound area (%) over 14 d using the macroscopic wound images. D) Immunostaining of the wound sections for cytokeratin to visualize the epidermal regrowth following wounding. "W" refers to the initial wound and "F" refers to the subcutaneous fat area. The edge of the fat layer marks the wound edge. Bar = 250 μ m. E) Quantification of the regrowth of the epidermis beyond the wound edge in various treatment groups. F) Histological sections from the wounds in ob/ob mice after 14 d with treatment with syndesomes (S4PL) and FGF-2. The sections were stained with Movat's pentachrome stain. Bar = 1 mm. *Statistically different from all treatment groups (p < 0.05; n = 8).



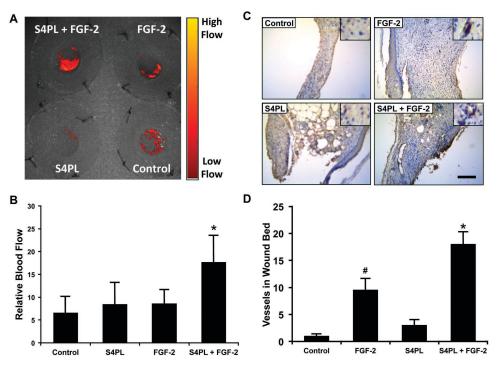


Figure 5. Syndesomes increase perfusion in the developing wound beds. A) Laser speckle contrast image of the dorsal surface of the mice with the four wounds 7 d postsurgery and a heat map showing relative blood flow. B) Quantification of blood flow in the wounds at day 7, relative to perfusion on the day of surgery. C) Histological sections of wound bed after 14 d after wounding immunostained for an endothelial marker (von Willebrand factor). Bar = 125 μ m and insets are magnified 1.5 times. D) Quantification of the number of vessels per field of view in the wound bed for different treatment groups. *Statistically different from all other groups (p < 0.05; n = 8). *Statistically different from the control and S4PL groups (p < 0.05; n = 8).

2.7. Syndesomes Enhance Wound Healing Phenotype in Macrophages

Macrophages are key players in the wound healing cascade through the regulation of inflammation and healing responses. Macrophages can express a continuum of phenotypes that are often broadly classified into M1 macrophages with pro-inflammatory activities or M2 macrophages that orchestrate matrix deposition and wound healing. We examined the expression of CD86 (M1 marker) and CD163 (M2 marker) using immunostaining of histological sections from the mice treated with syndesome-incorporating alginate wound dressings after 14 d. This analysis demonstrated a decrease in the expression of CD86 with syndesome treatment (Figure 6A,B). In addition, the levels of the M2 marker CD163 were increased in the wound beds (Figure 6C,D). Interestingly, the modulation of the marker expression was present in both the syndesomes with FGF-2 and in the S4PL alone groups, suggesting that the syndesomes were directly inducing immunomodulation in the wounds.

To further examine whether syndesomes could modulate the immune response during healing, we treated ob/ob mice with the various wound dressings and harvested the wound tissues at two and six days following wounding. We digested half of the harvested wound beds into a single cell suspension and used flow cytometry to quantify the expression of macrophage markers. Six days after wounding, we found a decreased number of macrophages (F4/80⁺ cells) and increased expression of the M2 marker CD206 in the syndesomes with FGF-2 treated wounds in comparison to FGF-2 only treated wounds (Figure 6E,F). We took the other half of the wound bed from day two and six after wounding, lysed the tissue, and performed an analysis of the cytokines in the wound using ELISA and cytokine antibody arrays. The cytokine antibody array at day 6 revealed many changes in the cytokine concentrations compared to the control group (Figure 6G and Figure S6, Supporting Information). The ELISA revealed similar levels of IL-1 α , an inflammatory cytokine released by many cell types including neutrophils and macrophages, between the four treatment groups (Figure 6H). We also observed an increase in IL-4 and IL-6 in the syndesomes with FGF-2 treated wounds over FGF-2 alone treated wounds (Figure 6I,J). Both of these cytokines have been linked to alternative activation of macrophages and this finding is consistent with the increased CD163 expression and decreased CD86 expression in the syndesomes with FGF-2 treatment group. In addition, there were increased levels of stromal cell-derived factor-1 (SDF-1), IL-1 β , monokine induced by gamma interferon (MIG/CXCL9), and IL-2 in the syndesomes with FGF-2 group versus wounds treated with FGF-2 alone (Figure S7 and Table S3, Supporting Information). Previous studies have shown that exogenously applied SDF-1 or IL-2 enhances wound healing.^[16] A proteomic analysis of chronic pressure ulcers in human patients found that MIG increases in chronic ulcers that heal but remains constant in those that do not heal.^[17]





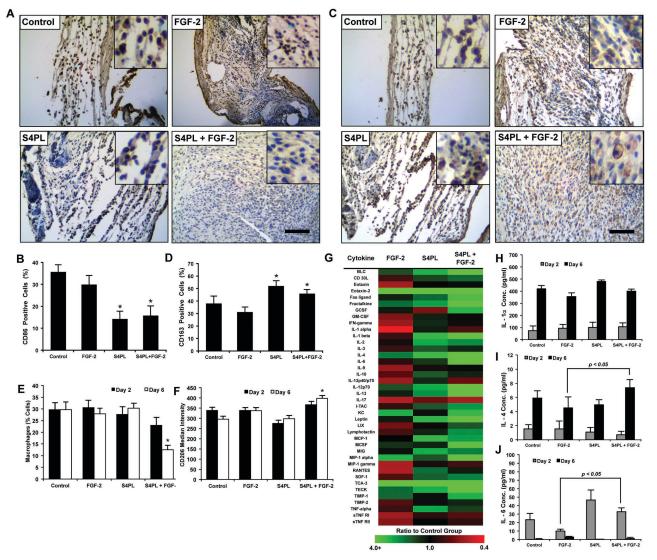


Figure 6. Syndesomes temporally modulate the macrophage response to wound healing phenotype. A) Histological sections of the wound beds 14 d postsurgery with immunostaining for an M1 macrophage marker (CD86). Bar = 125 μ m and insets are magnified threefold. B) Quantification of CD86 positive cells within the wound beds. **p* < 0.05 versus FGF-2 group (*n* = 8). C) Histological sections of the wound beds 14 d postsurgery with immunostained for an M2 macrophage marker (CD163). Bar = 125 μ m and insets are magnified threefold. D) Quantification of the number of CD163 positive cells in the wound beds. **p* < 0.05 versus FGF-2 group (*n* = 8). E) Analysis of cells harvested from wounds in ob/ob mice after 2 or 6 d postsurgery using flow cytometry. Cells were stained for macrophage marker (F4/80) and compared to the total cells measured in the wound. **p* < 0.05 versus all other groups at day 6 (*n* = 5). F) Median intensity of staining for M2 macrophage marker (CD206) in macrophages harvested from wounds 2 or 6 d postsurgery using flow cytometry. **p* < 0.05 versus all other groups at day 6 (*n* = 5). G) Heat map image of the fold change (compared to control group) in the concentration of various cytokines in the wounds 6 d after surgery. H–J) Concentrations (pg mL⁻¹) of IL-1*a*, IL-4, and IL-6, respectively, in the wound bed at days 2 and 6 measured using ELISA normalized to the total protein concentration. **p* < 0.05 versus the FGF-2 group (*n* = 5).

3. Discussion

Clinical trials using growth factor therapies to enhance diabetic wound healing have produced poor or equivocal results.^[8] Here, we hypothesized that the current approach of delivering growth factors is not effective because it does not account for the changes in tissue responsiveness due to disease. We examined skin samples from patients with type 2 diabetes and found that the levels of syndecan-4 were reduced in both the overall skin and blood vessels relative to nondiabetic patients. We then tested the ability of syndecan-4 liposomes in controlling wound

healing in in vitro and in vivo studies. Overall, the delivery of syndecan-4 protein with FGF-2 markedly improves many indices of wound healing including the migration of keratinocytes, wound closure, and shifting the macrophages toward the wound healing M2 phenotype (**Figure 7**). In addition, our results support the validity of the concept that by delivering coreceptors downregulated by a disease state, one can markedly improve the efficacy of a delivered therapeutic ligand.

A key point of our study is that the diabetic disease state must be considered when developing protein therapeutics for wound healing. Many clinical trials have been performed for therapies



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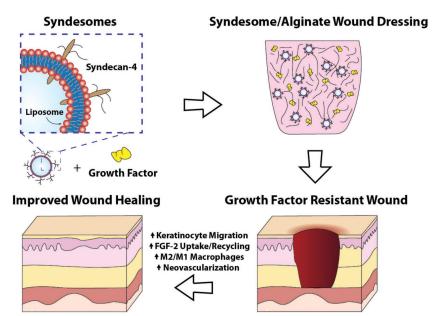


Figure 7. Summary diagram of the findings of the study and the enhancing activity of the syndesomes.

to improve the healing of chronic wounds based on the findings in large animal models in the absence of diabetics. In fact, the most commonly used preclinical wound model is performed in the nondiabetic pig, a model that has relatively rapid wound healing and does not have healing resistant wounds. Our findings that diabetic patients have reduced syndecan-4 in blood vessels of the skin illustrates the profound difference that exists between healthy patients and those that are prone to developing chronic wounds. We hypothesize that much of this loss of syndecan-4 can be attributed to the shedding and degradation of the protein by diabetes-induced changes in protease activity. This hypothesis is supported by the loss of the glycans observed in diabetes^[18] and that syndecan-4 is shed by factors increased in diabetes including reactive oxygen species,^[19] proteases,^[20] and inflammation.^[21] This concept is also supported by our prior studies in diabetic mice in which we found a significant reduction in many of the growth factor receptors and co-receptors in the skeletal muscle and myocardium.^[10] Therefore, we would argue that it is essential to perform preclinical studies for wound healing in animal models that represent the disease states that commonly accompany nonhealing wounds in patients. As diabetic porcine models have been used extensively in the study of atherosclerosis,^[11] it would seem that there is both an economic and ethical imperative to use these types of model in preclinical studies of wound healing to reduce the risk of failed clinical trials.

While previous studies have shown endogenous syndecan-4 plays a role wound healing, it is surprising that delivery of exogenous syndecan-4 protein is able to enhance keratinocyte migration and wound healing to the extent we observed in our studies. Syndecan-4 is induced in the skin following acute wounding in both mice and neonatal humans.^[22] Mice lacking syndecan-4 have delayed wound healing and impaired angiogenesis.^[23] Therefore, in the context of wound healing there are likely multiple benefits to increasing syndecan-4 in the wound

bed. Several prior studies have also supported a role for syndecan-4 in wound healing independent of its activity as a co-receptor for FGF-2. Endogenous syndecan-4 expression promotes fibroblast migration and regulates integrin signaling and small GTPases during wound healing.^[24] In addition, syndecan-4 also enhances keratinocyte migration^[25] and is necessary for migration of fibroblasts in fibrin gels.^[26] Our previous work has shown that delivery of syndecan-4 in a proteoliposome was more potent in inducing cell proliferation/migration, activation of ERK1/2 signaling pathway, in vitro endothelial tube formation, nuclear trafficking of growth factors, and angiogenesis in comparison to the free syndecan-4 protein.[46] In our studies showed increased migration in keratinocytes and decreased invasion activity when the cells were treated with exogenous syndecan-4 protein in a proteoliposome. This would suggest that the developed treatments would be able to synergistically enhance cell therapies, including those delivered from electrospun

materials.^[27] With exogenous delivery of the protein there is the possibility that the syndecan-4 works as a competitive inhibitor to the binding of the endogenous syndecan-4. Whether this occurs is likely a function of concentration of the ligand bound by syndecan-4, the concentration of the relevant receptor and the concentration of endogenous syndecan-4. In this case, it would suggest there is additional capability in keratinocytes to have enhanced FGF-2 signaling through the addition of syndecan-4 but that additional syndecan-4 serves as a competitive inhibitor for fibroblasts undergoing invasion.

Our current study suggests that a major activity of syndesomes is to enhance FGF-2 recycling through endosome-mediated mechanisms. Syndecan-4 is a key co-receptor in the FGF-2 and FGFR-1 signaling cascade^[28] where the heparan sulfate chains bind to FGF-2, and syndecan-4 dimerizes to aid as a coreceptor to FGFR-1. Furthermore, FGF-2 and FGFR-1 reside in the same endosomal compartment as syndecan-syntenin-PIP2 complex.^[29] Both FGF-2 and FGFR-1 are taken up through the clathrin-mediated pathway, followed by trafficking to the early and late endosomes.^[30] Syndecan-4 also recycles to the surface through both early and late endosomes^[31] In our studies, we found significantly higher amounts of FGF-2 in the early endosomes (Rab5 positive). This finding would be expected with overexpression of the syndecan-4 gene, as an increased amount of syndecan-4 would facilitate receptor binding and uptake through pinocytosis.^[32] However, as the proteoliposomes used do not undergo direct membrane fusion it is less clear how these changes might occur with syndesome treatment. We hypothesize that syndesomes increase FGF-2 uptake by enhancing the binding of FGF-2 to its receptor through the heparan sulfate chains of syndecan-4 and then facilitating the uptake of additional FGF-2 bound to syndecan-4 in the liposomal membrane during internalization. This hypothesis is consistent with our previous finding that free syndecan-4 is not as effective in enhancing FGF-2 uptake, signaling and

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angiogenesis.^[46] It would also be consistent with our finding of increased recycling of FGF-2 through the slow (Rab11) and fast (Rab4) mechanisms that we observed in our studies. This increased recycling may be the result of FGF-2 bound syndecan-4 being trafficked back to the surface after being internalized through the syndesome construct. This recycled FGF-2 would therefore be available for additional receptor interactions,^[33] making the FGF-2 more effective for an equivalent dose and leading to a prolonged effect.

Our study supports that the delivery of exogenous syndecan-4 protein drives wound macrophages toward the M2 phenotype. Wound healing is a delicate balance between the necessary inflammation that facilitates wound closure and angiogenesis, and excessive inflammation that can impede the wound healing process. A recently proposed scheme classifies macrophages as ranging in a phenotypic continuum from inflammatory (M1) to "alternatively activated" (M2) phenotypes.[34] However, the exact nature of these phenotypic states remains unclear and multiple other sub-phenotypes have been hypothesized. Efficient wound healing requires both the necessary inflammatory state and the pro-fibrotic, scaffold generating state. Thus, one hypothesis is that chronic nonhealing wounds can arise when too much or too little inflammation is present, and scar formation can occur when the "healing" response is overactive and leads to wound fibrosis and scarring.^[35] Within the wound environment, various subsets of macrophages have been associated with inflammation or with fibrosis but the strict definitions of M1 and M2 phenotypes do not adequately characterize the full complexity of wound macrophage phenotypes.^[36]

The detailed mechanistic role of syndecan-4 in macrophage phenotype is unknown but several studies support that it is functionally involved in LDL uptake,^[37] signaling in response to RANTES and SDF-1,^[38] and the response to endotoxic shock.^[39] Our study demonstrated increased M2 macrophage phenotype at early time points in the wounds, suggesting that syndesomes can alter the initial immune response to the wound. The presence of increased M2 macrophages would have a number of benefits for healing in chronic wounds including enhancing angiogenesis and the production of pro-healing cytokines.^[40] Consistent with M2 macrophage phenotype, we observed an increase in cytokines associated with M2 macrophages (IL-4 and IL-6) as well as a number of pro-healing cytokines including IL-2 and SDF-1. Topically applied IL-4 can increase wound healing in mice and facilitated macrophage differentiation into the M2 phenotype.^[41] IL-6 is also essential for wound healing and facilitates keratinocyte migration, wound contraction and macrophage infiltration.^[42] In addition, both IL-2 and SDF-1 have been shown to increase wound healing in small animal models.^[16] Thus, our studies demonstrate that syndesomes act in the early stages of wound healing to enhance the production of pro-healing cytokines including those that would facilitate an M2 macrophage phenotype.

4. Conclusions

In summary, we have shown that there is a reduction of syndecan-4 protein in diabetic patients and that syndesomes enhance FGF-2 therapy in the context of wound healing in



the diabetic disease state. Our studies support that the syndesomes increase keratinocyte migration, endosomal recycling of FGF-2, and enhance the M2 macrophage phenotype and production of pro-healing cytokines. While it is likely that there exist many other mechanisms of growth factor resistance diabetes it is encouraging that significant improvements in therapeutic potential can be garnered by targeting only the FGF-2/ syndecan-4 signaling pathway. Further studies are needed to both understand the detailed mechanisms of growth factor resistance and to further develop therapeutics to be effective in disease states. In this context, our therapeutic paradigm of delivering co-receptors as enhancers of growth factor activity may be applicable to a number of other biological systems in which disease modifies the responsiveness of the tissue such has hyperlipidemia and metabolic syndrome.

5. Experimental Section

Human Samples: Human skin samples were obtained from the Glasgow Caledonian University Skin Research Tissue Bank, Glasgow, UK. The tissue bank has National Health Services (NHS) research ethics approval to supply human skin for research (REC REF: 11/S1402/2). The samples were already paraffin embedded before being shipped to the authors. The samples were sectioned using a microtome to obtain 6 μ m thick sections. The slides were for syndecan-4 (Abcam) using the Envision+ Dual Link Kit (Dako). The details of the staining procedure are described in a later section. Nine samples were used in both diabetic and nondiabetic groups.

Recombinant Syndecan-4 Protein Production: HEK293-T cells were transduced with a custom made plasmid with full-length syndecan-4 gene using a lentiviral transduction system. The syndecan-4 overexpressing stable cells were grown in high glucose Dulbecco's Modified Eagle Medium (DMEM) with 10% fetal bovine serum (FBS), 5% penicillinstreptomycin, and 5% L-glutamine. The cells were lysed using a lysis buffer containing 1% Triton X-100 and protease inhibitors (Roche). The cell lysate was sonicated, vortexed, and then centrifuged (25 000× g). The supernatant was used for protein purification by a HiTrap Q HP column (GE Healthcare) using Fast Protein Liquid Chromatography (FPLC; Amersham Biosciences). Pure protein was confirmed by silver stain and a western blot probing for the syndecan-4 protein, and the protein concentration was quantified using a bicinchoninic acid (BCA) assay (Thermo Scientific).

Preparation of Syndesomes: The lipids used for the preparation were 1,2-dioleoyl-sn-glycero-3-phosphocholine (DOPC), 1,2-dioleoylsn-glycero-3-phosphoethanolamine (DOPE), cholesterol, and sphingomyelin (Avanti Polar Lipids). Briefly, a solution mixture of the four lipids at 10 mg mL⁻¹ concentration was made in a volumetric ratio of 2:1:1:1 chloroform. The mixture was prepared in a round bottom glass flask and the chloroform was removed using a rotatory evaporator for 1 h followed by treatment with stream of argon gas for 15 min. Once all the chloroform was removed, the lipid film was resuspended in a HEPES-buffered salt solution by vortexing, sonicating, and freeze thawing three times each in order. This lipid solution was then extruded through a 400 nm polycarbonate membrane filter (Avestin) to generate liposomes. Syndecan-4 protein was added to the liposome suspension to a final concentration of 50 μg mL^-1. To this solution, 1% n-octyl- β -D-glucopyranoside was added to permeablize the liposomes and incorporate the protein. The detergent was then removed through serial dilution, extensive dialysis, and treatment with BioBeads (SM-2, Bio-Rad). The amount of protein incorporated into the liposomes was measured using a BCA assay (Thermo Scientific). FGF-2 (Peprotech) was mixed with the syndesomes when they needed to be delivered together.

Liposome Characterization: The size and dispersion of the syndesomes and isolated syndecan-4 was characterized by dynamic light scattering



(Malvern Zetasizer Nano ZS). The instrument was calibrated using 54 nm diameter polystyrene particles. The syndesomes were diluted 1:1000 to fit the detection region of the instrument and then aliquoted into a polystyrene cuvette to run in the machine. The results were an average of 50 size measurements. For imaging with cryo-electron microscopy, the liposomes were plunge-frozen in liquid ethane on carbon holey film grids as previously described (R2×2 Quantifoil; Micro Tools GmbH, Jena, Germany).^[43] The grids were transferred to a cryo-specimen holder (Gatan 626) under liquid nitrogen and put in a microscope (JEOL 2100 LaB6) operating at 200 keV. Grids were maintained at close to liquid nitrogen temperatures during EM session (–172 to –180 °C). Liposomes were (UltraScan 895, GATAN, Inc.) using low-dose imaging procedure. Images were acquired with less than 20 electrons Å⁻² electron dose.

Preparation of Syndesome-Releasing Alginate Gels: We created a 6.35 mm diameter alginate disk using a custom-designed mold to implant in the wound. Equal volumes of 4% sodium alginate (Sigma) solution and 0.85% NaCl solution were mixed and the syndesomes and/or FGF-2 were added to this solution. The alginate solution was pipetted into the mold and then cross-linked with a solution of 1.1% CaCl₂ for 1 h at 4 °C. We used 5 μ g of FGF-2 and/or 0.5 μ g of syndecan-4 protein according to the sample (control, FGF-2, S4PL, or S4PL with FGF-2) in each disk implanted. For the release studies, two alginate disks with different treatments were placed in a scintillation vial containing 10 mL of 1× PBS with Ca^{2+} and Mg^{2+} . At every time point, 200 μ L of buffer was aliquoted from the scintillation vial and frozen while replacing 200 μ L of fresh buffer into the vial. The buffer samples at each time point were analyzed using FGF-2 ELISA for the amount of FGF-2 released cumulatively over the course of a week. The alginate disks were flash frozen in liquid nitrogen (–195 $^\circ\text{C})$ and lyophilized overnight (-110 °C, 0.0005 mbar) in scintillation vials. The final freeze-dried gels were sputter coated with gold discharge for 30 s and then imaged using the scanning electron microscope (FEI Quanta 650 ESEM) at 10 kV.

Electric Cell-Substrate Impedance Sensing (ECIS) Assay for Cell Migration: The cells used for the assay were adult dermal fibroblasts and adult epidermal keratinocytes, both from either healthy or type 2 diabetic donors (Lonza). Fibroblasts were grown in high glucose DMEM (Gibco) with Pen-Strep, 10% FBS, L-glutamine, and fibroblast supplements (Lonza) while the keratinocytes were grown in MCDB-131 (Gibco) with Pen-Strep, 10% FBS, L-glutamine and keratinocyte supplements (Lonza). However, when the cells were used for the experiment, the media was serum free. The 96W1E+ plates (96 wells) were first coated with 100 µL of 2×10^{-3} M Cysteine (Sigma) per well for 30 min followed by a quick wash with $1 \times$ PBS. The wells were then coated with 40 µL per well of fibronectin (Sigma) at 8 μ g mL⁻¹ overnight. After a quick 1× PBS wash, to remove unbound fibronectin, the cells were plated at 10 000 cells per well and allowed to attach, while the plate was placed on the Z-Theta instrument (ECIS), which created an electric fence around the electrode. The cells were allowed to settle and attach for 4 h. Finally, the electric fence was turned off and the cells were allowed to migrate over the electrode. The substrate impedance and resistance were measured every 48 s at a frequency of 40 000 Hz. Six wells per treatment group in the migration assay were used.

Fibroblast Invasion Assays: Human adult dermal fibroblasts (Lonza) were used in the Trevigen Inc. The fibroblasts were cultured in with high glucose DMEM with Pen-Strep, 10% FBS, L-glutamine, and fibroblast supplements (Lonza). The cells were starved for 24 h in media without serum before the assay in high glucose DMEM with Pen-Strep, L-glutamine (no FBS). The treatments were added to this starvation media. Collagen-I cell invasion assay to assess the invasion potential of the fibroblasts in the presence of various treatments. The top invasion chamber was coated with collagen I and kept to attach overnight. The cells were plated in each well at a concentration of 10^6 cells mL⁻¹ in the top chamber and treatments were added to the bottom chamber. The cells were incubated with the treatments for 24 h and then the top chambers were moved to the assay plate with Calcein-AM and cell dissociation solution. This solution detaches the cells that have invaded from the top chamber to the bottom side. Finally,

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the assay plate was read without the top chamber at 485 nm excitation and 520 nm emission. The intensity is a measure of the amount of cell invasion through the collagen I layer. Six wells per treatment group in the invasion assay were used.

Intracellular Trafficking of FGF-2 Using Co-Localization With Rab Adapter Proteins: The Rab5-GFP, Rab7-GFP, and Rab11-GFP plasmids were provided by Dr. Mukhopadhyay and have been previously described.^[44] The Rab4-GFP and Rab9-GFP constructs were purchased from Addgene.^[45] FGF-2 (Peprotech) was conjugated with Alexa Fluor 594 (Life Technologies) using the heparin column that binds the active site of FGF-2 preserving its biological activity.^[10,46] HEK293Ta cells plated on 8-well glass slides (ibidi) at 10 000 cells per well and were transfected with the above-mentioned plasmids using DNA HTS jetPEI transfection reagent (Polyplus transfection) using standard protocol. Twenty four hours posttransfection, the cells were treated with AF594 tagged FGF-2 (1 $\mu L)$ and/or syndesomes (1 $\mu L).$ The cells were fixed at 15, 30, 60, and 120 min using 4% paraformaldehyde (Electron Microscopy Sciences) and washed three times with PBS for 10 min each. The cell nuclei were stained with DAPI (Vector Labs) and mounting media was added in the wells. The slides were then imaged using the laser scanning confocal microscope (Zeiss LSM710). The percentage of Rab-GFP labeled endosomes containing AF594 tagged FGF-2 was calculated as follows: each cell was divided into four roughly equal quadrants and one of the quadrants was chosen for quantification randomly (using RAND function of Excel). The total number of Rab-GFP labeled endosomes and endosomes that co-localize with AF594 tagged FGF-2 in the chosen quadrant were counted to calculate the percentage of co-localization. For each time point and treatment group, 10 cells were analyzed using Metamorph (Molecular Devices).

Animal Studies: All animal experiments were performed with the approval of the Institutional Animal Care and Use Committee (IACUC) of University of Texas at Austin, and in accordance with NIH guidelines "Guide for Care and Use of Laboratory Animals" for animal care. All the animal experiments were performed on a diabetic, obese, and hyperlipidemic mouse model (ob/ob). All the ob/ob mice (B6. Cg-Lep^{ob}/J) were purchased from the Jackson Laboratory. All animals were fed a high fat diet (Research Diets – D12331) for 10 weeks before performing wound healing surgeries.

Excisional Wound Healing Model: To examine wound healing in the diabetic and obese mice, we used a full-thickness excisional model with a splint to prevent wound contraction.^[47] A sterile 5 mm biopsy punch was used to outline a pattern of four wounds, two on either side of midline on the dorsum of the mouse. A splint was fashioned using 0.5 mm thick silicone sheet and was placed so that the wound was centered within the splint. The splint was immobilized in place using 6-0 nylon sutures and cyanoacrylate glue to prevent wound contraction. Alginate gel disks encapsulating syndesomes and/or FGF-2 were then applied directly to the region of the open wound. A single sheet of Tegaderm was used to cover all the wounds. Photographs of the wounds were taken on days 0, 7, and 14. The animals were euthanized at 2, 6, and 14 d, and the wounds were biopsied with a 10 mm biopsy punch. The tissues were snap frozen in liquid N₂-chilled isopentane and used for further analysis.

Laser Speckle Contrast Imaging of Tissue Perfusion: A custom laser speckle contrast imager was used to image the tissue blood flow as previously described.^[48] Briefly, a near infrared (785 nm, 50 mW) laser diode (Thor Labs) was used to illuminate the wounds on the back, and the speckle was captured using a Zoom-7000 lens (Navitar) linked to a Bassler CCD camera (Graftek). The wounds were imaged right after surgery (day 0), and at day 7. All wounds were imaged simultaneously within the laser field to allow the quantification of relative perfusion.

Histological Analysis and Immunostaining: Tissues from the in vivo experiments were embedded in paraffin and 6 μ m thick sections were produced using a microtome. The slides were stained with H&E or Movat's pentachrome stains. The wound healing samples were also immunostained using the Envision+ Dual Link Kit (Dako North America, Inc.) for cytokeratin (Abcam), CD86 (Bioss), CD163 (Bioss), or von Willebrand factor (Dako). The details about the antibodies are mentioned in Table S2 in the Supporting Information. Briefly, the slides



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were de-paraffinized and placed in a bucket with Antigen Retrieval Solution (Dako), and placed in the microwave (1250 W) for 2 min and 40 s. Then the bucket was placed in a water bath maintained at 80 °C for 3 h. This reduces the background staining significantly. The slides were cooled in solution for 20 min and washed in PBS twice for 5 min each. Then, they were blocked in 20% fetal bovine serum in PBS for 45 min at room temperature. The slides were then washed two times for 5 min in PBS and a circle was drawn around the section with a hydrophobic pen. The sections were peroxide blocked with dual enzyme block solution (Dako) and incubated for 30 min. This was followed by three washes in PBS for 5 min each. After that, the primary antibody in antibody diluent (Dako) was applied to the sections and the slides were incubated at 4 °C for overnight. On the following day, the sections were washed in PBS thrice and then the peroxidase labeled polymer (HRP) was added and the slides were incubated for 30 min at room temperature. Following the incubation, nine washes with PBS were done after with a wait of 5 min after every three washes. In the meantime, the DAB+ solution was prepared and added to the sections once washing had been completed. The incubation period was optimized according to the intensity of staining. After three washes in PBS, the slides were stained in Mayer's Hematoxylin for 3 min. Finally, they were washed in distilled water three times, mounted with an aqueous mounting media and covered with a cover glass. For each treatment group we analyzed five slides per sample

(total 40 slides) each with 2-3 sections. Wound Digestion and Flow Cytometry Analysis: The wounds (days 2 and 6) were excised out using a 10 mm sterile biopsy punch and cut from the center into two disc-shaped pieces. Half of the tissue was used for cryosectioning and histology. The other half was digested^[49] in an enzyme cocktail and used for the flow cytometry experiments. The single cell suspension from the wound tissue was maintained at 10^6 cells mL⁻¹ in the FACS staining buffer (BD). The samples were blocked with 1 $\mu g\ m L^{-1}$ (final concentration) of Rat IgG_{2b} for 20 min on ice. The cells were then stained with the following antibodies for 30 min on ice: anti-mouse F4/80 (Pe-Cy7), anti-human CD206 (FITC), and anti-mouse CD86 (Biotin; refer Table S2, Supporting Information for additional antibody details). Two washes were performed with FACS staining buffer. The PerCP streptavidin antibody was used to stain the samples for another 20 min on ice. The samples were finally washed twice with the FACS staining buffer and resuspended in 1 mL buffer. The samples were fixed with 500 µl of cytofix buffer (BD Biosciences) and stored at 4 °C. The samples were run together on the BD LSRFortessa cell analyzer recording at least 10,000 events in every sample. The final data were analyzed using FlowJo software (FlowJo, LLC).

Quantification of Wound Closure and Immunohistochemical Staining: The macroscopic pictures of the wounds taken during surgery at days 0, 7, and 14 were used for the wound closure analysis. The Meiji stereozoom surgical dissection microscope with a Nikon D70 camera was used to take the pictures of the wounds. The camera height was fixed throughout the experiment and the inner diameter of the silicone splints (6 mm) served as the parameter to normalize the wound area. The images were quantified using Metamorph (Molecular Devices) and were compared to the day 0 area (100% open). The immunostained slides were imaged using a Meiji brightfield microscope with CCD camera at 10×, 20×, and 40× magnifications. The images from each treatment group with five sections were used for the quantification. The number of cells that were positively stained was quantified in comparison to the total cells.

Measurement of Cytokines in Wound Lysates: The wound tissues were frozen in liquid N₂ cooled isopentane. The samples were sectioned into 1 µm thick sections using a cryostat. The sections were solubilized using the lysis buffer with 1% Triton-X 100 and protease inhibitors. The lysate was centrifuged at 25,000g in a refrigerated centrifuge and the supernatant was applied to a Ray Biotech Mouse Inflammation Antibody Array 1 (G-series). The arrays were processed according to the manufacturer's instructions. The images were scanned using a laser scanner with the Cy3 channel. The intensity data were background subtracted with the negative controls and normalized with respect to the positive controls.

Statistical Analysis: Comparisons between two groups were performed using a two-tailed Student's *t*-test. Multiple comparisons between groups were analyzed by two-way ANOVA followed by a two-sided Dunnett post-hoc testing. For the wound closure data, the test groups compared with a two-tailed *p*-value of <0.05 were considered as statistically significant.

Supporting Information

Supporting Information is available from the Wiley Online Library or from the author.

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- [1] N. Singh, D. G. Armstrong, B. A. Lipsky, JAMA 2005, 293, 217.
- [2] a) A. American Diabetes, *Diabetes Care* 2013, 36, 1033;
 b) J. Larsson, C. D. Agardh, J. Apelqvist, A. Stenstrom, *Clin. Orthop. Relat. Res.* 1998, 350, 149.
- [3] R. Goldman, Adv. Skin Wound Care 2004, 17, 24.
- [4] L. K. Branski, C. T. Pereira, D. N. Herndon, M. G. Jeschke, *Gene Ther.* 2007, 14, 1.
- [5] P. Zahorec, J. Koller, L. Danisovic, M. Bohac, Cell Tissue Bank 2015, 16, 19.
- [6] B. Buchberger, M. Follmann, D. Freyer, H. Huppertz, A. Ehm, J. Wasem, Exp. Clin. Endocrinol. Diabetes 2011, 119, 472.
- [7] a) A. Bhansali, S. Venkatesh, P. Dutta, M. S. Dhillon, S. Das, A. Agrawal, *Diabetes Res. Clin. Pract.* 2009, *83*, e13; b) R. C. Fang, R. D. Galiano, *Biologics* 2008, *2*, 1; c) J. M. Smiell, T. J. Wieman, D. L. Steed, B. H. Perry, A. R. Sampson, B. H. Schwab, *Wound Repair Regen.* 1999, *7*, 335; d) D. L. Steed, *J. Vasc. Surg.* 1995, *21*, 71; e) T. J. Wieman, J. M. Smiell, Y. Su, *Diabetes Care* 1998, *21*, 822.
- [8] a) J. B. Acosta, W. Savigne, C. Valdez, N. Franco, J. S. Alba, A. del Rio, P. Lopez-Saura, G. Guillen, E. Lopez, L. Herrera, J. Fernandez-Montequin, Int. Wound J. 2006, 3, 232;
 b) J. I. Fernandez-Montequin, B. Y. Betancourt, G. Leyva-Gonzalez, E. L. Mola, K. Galan-Naranjo, M. Ramirez-Navas, S. Bermudez-Rojas, F. Rosales, E. Garcia-Iglesias, J. Berlanga-Acosta, R. Silva-Rodriguez, M. Garcia-Siverio, L. H. Martinez, Int. Wound J. 2009, 6, 67;
 c) V. K. Mohan, Diabetes Res. Clin. Pract. 2007, 78, 405;
 d) J. L. Richard, C. Parer-Richard, J. P. Daures, S. Clouet, D. Vannereau, J. Bringer, M. Rodier, C. Jacob, M. Comte-Bardonnet, Diabetes Care 1995, 18, 64.



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- [9] a) J. C. Fiddes, P. A. Hebda, P. Hayward, M. C. Robson, J. A. Abraham, C. K. Klingbeil, *Ann. N. Y. Acad. Sci.* **1991**, *638*, 316;
 b) S. E. Lynch, R. B. Colvin, H. N. Antoniades, J. Clin. Invest. **1989**, *84*, 640.
- [10] S. Das, G. Singh, A. B. Baker, Biomaterials 2014, 35, 196.
- [11] A. B. Baker, Y. S. Chatzizisis, R. Beigel, M. Jonas, B. V. Stone, A. U. Coskun, C. Maynard, C. Rogers, K. C. Koskinas, C. L. Feldman, P. H. Stone, E. R. Edelman, *Atherosclerosis* **2010**, *213*, 436.
- [12] a) A. B. Baker, W. J. Gibson, V. B. Kolachalama, M. Golomb, L. Indolfi, C. Spruell, E. Zcharia, I. Vlodavsky, E. R. Edelman, J. Am. Coll. Cardiol. 2012, 59, 1551; b) A. B. Baker, A. Groothuis, M. Jonas, D. S. Ettenson, T. Shazly, E. Zcharia, I. Vlodavsky, P. Seifert, E. R. Edelman, Circ. Res. 2009, 104, 380.
- [13] R. Irschick, T. Trost, G. Karp, B. Hausott, M. Auer, P. Claus, L. Klimaschewski, *Histochem. Cell Biol.* 2013, 139, 135.
- [14] O. Seitz, C. Schurmann, N. Hermes, E. Muller, J. Pfeilschifter, S. Frank, I. Goren, *Exp. Diabetes Res.* 2010, 476969.
- [15] V. van Weel, M. de Vries, P. J. Voshol, R. E. Verloop, P. H. Eilers, V. W. van Hinsbergh, J. H. van Bockel, P. H. Quax, Arterioscler. Thromb. Vasc. Biol. 2006, 26, 1383.
- [16] a) A. Barbul, J. Knud-Hansen, H. L. Wasserkrug, G. Efron, J. Surg. Res. **1986**, 40, 315; b) X. Xu, F. Zhu, M. Zhang, D. Zeng, D. Luo, G. Liu, W. Cui, S. Wang, W. Guo, W. Xing, H. Liang, L. Li, X. Fu, J. Jiang, H. Huang, *Cells Tissues Organs* **2013**, *197*, 103.
- [17] L. E. Edsberg, J. T. Wyffels, M. S. Brogan, K. M. Fries, Wound Repair Regen. 2012, 20, 378.
- [18] A. H. Salmon, S. C. Satchell, J. Pathol. 2012, 226, 562.
- [19] A. Singh, R. D. Ramnath, R. R. Foster, E. C. Wylie, V. Friden, I. Dasgupta, B. Haraldsson, G. I. Welsh, P. W. Mathieson, S. C. Satchell, *PLoS One* **2013**, *8*, e55852.
- [20] S. M. McCarty, S. L. Percival, Adv. Wound Care (New Rochelle) 2013, 2, 438.
- [21] R. Ramnath, R. R. Foster, Y. Qiu, G. Cope, M. J. Butler, A. H. Salmon, P. W. Mathieson, R. J. Coward, G. I. Welsh, S. C. Satchell, *FASEB J.* **2014**, *28*, 4686.
- [22] R. Gallo, C. Kim, R. Kokenyesi, N. S. Adzick, M. Bernfield, J. Invest. Dermatol. 1996, 107, 676.
- [23] F. Echtermeyer, M. Streit, S. Wilcox-Adelman, S. Saoncella, F. Denhez, M. Detmar, P. Goetinck, J. Clin. Invest. 2001, 107, R9.
- [24] a) M. D. Bass, R. C. Williamson, R. D. Nunan, J. D. Humphries, A. Byron, M. R. Morgan, P. Martin, M. J. Humphries, *Dev. Cell* **2011**, 21, 681; b) R. Brooks, R. Williamson, M. Bass, *Small GTPases* **2012**, 3, 73.
- [25] E. Araki, Y. Momota, T. Togo, M. Tanioka, K. Hozumi, M. Nomizu, Y. Miyachi, A. Utani, *Mol. Biol. Cell* **2009**, *20*, 3012.
- [26] F. Lin, X. D. Ren, G. Doris, R. A. Clark, J Invest. Dermatol. 2005, 124, 906.
- [27] a) A. Townsend-Nicholson, S. N. Jayasinghe, *Biomacromolecules* 2006, 7, 3364; b) S. N. Jayasinghe, *Analyst* 2013, 138, 2215.

- [28] a) A. Elfenbein, A. Lanahan, T. X. Zhou, A. Yamasaki, E. Tkachenko, M. Matsuda, M. Simons, *Sci. Signal.* 2012, *5*, ra36; b) A. Elfenbein, M. Simons, *J. Cell Sci.* 2013, *126*, 3799; c) A. Horowitz, E. Tkachenko, M. Simons, *J. Cell Biol.* 2002, *157*, 715; d) M. Simons, A. Horowitz, *Cell Signal* 2001, *13*, 855.
- [29] P. Zimmermann, Z. Zhang, G. Degeest, E. Mortier, I. Leenaerts, C. Coomans, J. Schulz, F. N'Kuli, P. J. Courtoy, G. David, *Dev. Cell* 2005, 9, 377.
- [30] S. Jean, A. Mikryukov, M. G. Tremblay, J. Baril, F. Guillou, S. Bellenfant, T. Moss, *Dev. Cell* 2010, 19, 426.
- [31] K. Lambaerts, S. A. Wilcox-Adelman, P. Zimmermann, Curr. Opin. Cell Biol. 2009, 21, 662.
- [32] E. Tkachenko, E. Lutgens, R. V. Stan, M. Simons, J. Cell Sci. 2004, 117, 3189.
- [33] B. Hausott, N. Vallant, M. Hochfilzer, S. Mangger, R. Irschick, E. M. Haugsten, L. Klimaschewski, *Eur. J. Cell Biol.* 2012, *91*, 129.
- [34] A. Sica, A. Mantovani, J. Clin. Invest. 2012, 122, 787.
- [35] S. K. Brancato, J. E. Albina, Am. J. Pathol. 2011, 178, 19.
- [36] J. M. Daley, S. K. Brancato, A. A. Thomay, J. S. Reichner, J. E. Albina, J. Leukoc. Biol. 2010, 87, 59.
- [37] B. B. Boyanovsky, P. Shridas, M. Simons, D. R. van der Westhuyzen, N. R. Webb, J. Lipid Res. 2009, 50, 641.
- [38] H. Slimani, N. Charnaux, E. Mbemba, L. Saffar, R. Vassy, C. Vita, L. Gattegno, *Biochim. Biophys. Acta* **2003**, *1617*, 80.
- [39] K. Ishiguro, T. Kojima, T. Muramatsu, Glycoconj. J. 2002, 19, 315.
- [40] N. Jetten, S. Verbruggen, M. J. Gijbels, M. J. Post, M. P. De Winther, M. M. Donners, Angiogenesis 2014, 17, 109.
- [41] V. Salmon-Ehr, L. Ramont, G. Godeau, P. Birembaut, M. Guenounou, P. Bernard, F. X. Maquart, *Lab. Invest.* 2000, *80*, 1337.
- [42] a) Z. Q. Lin, T. Kondo, Y. Ishida, T. Takayasu, N. Mukaida, *J. Leukoc. Biol.* **2003**, *73*, 713; b) M. M. McFarland-Mancini, H. M. Funk, A. M. Paluch, M. Zhou, P. V. Giridhar, C. A. Mercer, S. C. Kozma, A. F. Drew, *J. Immunol.* **2010**, *184*, 7219.
- [43] M. B. Sherman, R. H. Guenther, F. Tama, T. L. Sit, C. L. Brooks, A. M. Mikhailov, E. V. Orlova, T. S. Baker, S. A. Lommel, *J. Virol.* **2006**, *80*, 10395.
- [44] S. Mukhopadhyay, A. D. Linstedt, Proc. Natl. Acad. Sci. USA 2011, 108, 858.
- [45] a) A. Choudhury, M. Dominguez, V. Puri, D. K. Sharma, K. Narita, C. L. Wheatley, D. L. Marks, R. E. Pagano, J. Clin. Invest. 2002, 109, 1541; b) K. A. Rzomp, L. D. Scholtes, B. J. Briggs, G. R. Whittaker, M. A. Scidmore, Infect. Immun. 2003, 71, 5855.
- [46] E. Jang, H. Albadawi, M. T. Watkins, E. R. Edelman, A. B. Baker, Proc. Natl. Acad. Sci. USA 2012, 109, 1679.
- [47] X. Wang, J. Ge, E. E. Tredget, Y. Wu, Nat. Protoc. 2013, 8, 302.
- [48] A. B. Parthasarathy, W. J. Tom, A. Gopal, X. Zhang, A. K. Dunn, Opt. Express 2008, 16, 1975.
- [49] A. L. Brubaker, D. F. Schneider, J. L. Palmer, D. E. Faunce, E. J. Kovacs, J. Immunol. Methods 2011, 373, 161.